



## A jaw protruding dental splint improves running physiology and kinematics

Journal:	<i>International Journal of Sports Physiology and Performance</i>
Manuscript ID	Draft
Manuscript Type:	Brief Report
Date Submitted by the Author:	n/a
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Keywords:	occlusal splints, running economy, respiratory work, jaw advancement

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**1 Abstract**

2 Wearing an intraoral jaw protruding splint could enhance respiratory function in clinical  
3 settings and eventually exercise performance. **Purpose:** We studied the acute effect of  
4 wearing a lower jaw forwarding splint at different protruding percentages across a wide  
5 range of running exercise intensities. **Methods:** A case study was undertaken with a  
6 highly-trained and experienced 27 y old female triathlete. She performed an incremental  
7 intermittent treadmill running protocol on three occasions wearing three different  
8 intraoral devices (30 and 50% maximum range, and a control device) to assess running  
9 physiological and kinematical variables. **Results:** Both the 30 and 50% protruding splints  
10 decreased both the oxygen uptake and carbon dioxide production (by 4-12 and 1-10%,  
11 respectively), as well as increased the ventilation and respiratory frequency (by 7-12 and  
12 5-16%, respectively) during different exercise intensities. The exercise energy  
13 expenditure (~1-14%) and cost (7.8, 7.4 and 8.0 J·kg<sup>-1</sup>·m<sup>-1</sup> for 30 and 50%, and placebo)  
14 were also decreased. The triathlete's lower limbs running pattern changed by wearing the  
15 forwarding splints, decreasing the contact time and stride length by ~4%, and increasing  
16 the stride rate by ~4%. **Conclusions:** Wearing a jaw protruding splint can have a positive  
17 biophysical effect on running performance.

18 **Keywords:** occlusal splints, running economy, respiratory work, jaw advancement

19

## 20 Introduction

21 A mandibular protruding splint is a customized dental device that is worn intraorally  
22 to advance and hold the lower jaw in a forward position. These splints are used to  
23 increase the upper airway space and respiratory volumes<sup>1</sup>, and are now being  
24 manufactured specifically for sporting applications.<sup>2</sup> Increasing the upper airway  
25 volume, and reducing resistance to airflow passage, should increase ventilation and  
26 oxygenation, as well as lower the energy cost of breathing<sup>2,3</sup>. On this basis,  
27 manipulating the mandibular position has been evaluated as an intervention for  
28 enhancing aerobic performance via increased respiratory gas exchange.<sup>2,4</sup>

29 Despite the mechanical and potential respiratory benefits with wearing a protruding  
30 intraoral device, there are few reports to characterize its effect on exercise  
31 performance. Furthermore, since the available studies do not reveal the degree of  
32 forwarding jaw provided by the tested splints, it is unclear what degree of jaw  
33 advancement would be most effective in improving aerobic performance. The aim of  
34 this case study was to determine the acute effects of varying the degree of mandibular  
35 advancement on running performance.

## 36 Methods

### 37 Subjects

38 A well-trained female triathlete (Cross Triathlon World Champion 25-29 female y  
39 age group, height 1.67 m and body mass 56 kg) volunteered for this study and  
40 provided written informed consent after a full explanation of its purpose, benefits and  
41 risks. The experimental procedures were approved by the local University Ethics  
42 Committee (CEFADE282020) following the norms and standards of the Declaration  
43 of Helsinki.

### 44 Design

45 The triathlete visited the laboratory facilities on three occasions, 48 h apart, to  
46 complete an incremental intermittent treadmill running protocol until voluntary  
47 exhaustion. A different lower jaw splint was worn on each visit under randomized  
48 and single-blind conditions. The triathlete wore the same running shoes and clothing,  
49 was instructed to refrain from intensive training in the previous 24 h, and abstain from  
50 food, alcohol and caffeine in the 3 h before testing. Cardiorespiratory, metabolic and  
51 kinematic variables were recorded continuously throughout the incremental treadmill  
52 protocol, and continuous verbal feedback was provided for motivation.

### 53 Methodology

54 After the dental arch impressions were taken, two mandibular splints were custom  
55 manufactured to produce different jaw positions at 30 and 50% of the maximum range  
56 of the participant's protrusion (at a constant vertical dimension, Figure 1). A placebo  
57 splint was also produced that did not cover the occlusal teeth surfaces, nor changed  
58 the occlusion vertical dimension and mandibular position. All the intraoral splints  
59 were manufactured from thermoforming plates (Erkodur®, Germany) and checked  
60 for adaptability and comfortability.

61 Prior to each trial, the triathlete was familiarized with the specific splint and  
62 performed a 15 min warm-up run on the treadmill at low exercise intensity. The

63 experimental protocol consisted of 7 x 4 min running stages, 1 km·h<sup>-1</sup> increments and  
64 30 s rest periods on a motorized treadmill (AMTI, Watertown, USA).<sup>5</sup> Breath-by-  
65 breath responses were measured using a calibrated gas analyzer (K4b<sup>2</sup>, Cosmed,  
66 Rome, Italy), posteriorly smoothed by employing a moving and time average of three  
67 breaths and 5 s (respectively), with the last min of each stage being used for  
68 comparison between experimental conditions.<sup>5</sup> The maximal oxygen uptake ( $\dot{V}O_{2\max}$ )  
69 was determined using conventional physiological criteria<sup>5</sup>, and was always observed  
70 at the 7<sup>th</sup> stage of the protocol.

71 Capillary blood samples (5μl, Lactate Pro2, Arkay, Inc, Kyoto, Japan) were collected  
72 from a fingertip for measuring lactate concentration at rest, immediately after each  
73 stage and 3 min after the end of the protocol. The lactate-velocity curve was used to  
74 assess the anaerobic threshold (AnT)<sup>6</sup>, which was always observed at the 3<sup>rd</sup> running  
75 stage for all the trials. The energy expenditure was determined for each protocol stage  
76 and energy cost assessed as the slope of a regression line between the energy  
77 expenditure and the corresponding running velocities.<sup>5</sup>

78 Lower limb kinematic data were recorded from the right sagittal plane using a video  
79 camera (GoPro HERO6 Black, California, EUA) at a sampling rate of 60 Hz, fixed  
80 on a tripod placed 2 m from the treadmill and 1 m above the ground level. In each  
81 running stage, 10 consecutive strides were analyzed frame-by-frame using two-  
82 dimensional motion analysis software (Kinovea, v.0.8.27) to determine the contact  
83 and stride times, stride rate (1/stride time) and length (velocity/stride rate), as well as  
84 knee angular kinematics.

85 \*\*\*Figure 1\*\*\*

## 86 **Statistical analysis**

87 The statistical analyses were completed using IBM® SPSS® Statistics 27.0.1.0 (IBM  
88 Corp, USA). Mean and standard deviation were computed for all variables. A linear  
89 mixed effects model was performed with repeated measures analysis comprising both  
90 fixed (splint conditions) and random effects (changes over time). Significance  
91 accepted at p< 0.05.

## 92 **Results**

93 The assessed physiological and kinematical data are detailed in Table 1 and Figure 1  
94 (respectively) for each intraoral splint condition. When the protruding splints were  
95 used, oxygen uptake ( $\dot{V}O_2$ ) and carbon dioxide production ( $\dot{V}CO_2$ ) were ~4% lower,  
96 while the ventilation and respiratory frequency were higher (7-12 and 5-16%,  
97 respectively), across the different exercise intensities. For each protocol stage, the  
98 energy expenditure (~1-14%) and energy cost (7.8, 7.4 and 8.0 J·kg<sup>-1</sup>·m<sup>-1</sup> for 30 and  
99 50% and placebo) were lower when running with both protruding splints. Similarly,  
100 there were differences in the biomechanical variables in-between experimental  
101 conditions, with shorter contact times (~4%), higher stride rates (~4%) and lower  
102 stride lengths (~4%) when using the 30 and 50% splints.

103 \*\*\*Table 1\*\*\*

104

105 \*\*\*Figure 2\*\*\*

## 106 Discussion

107 The current results demonstrate that forwarding the jaw led to ~4% lower  $\dot{V}O_2$  and  $\dot{V}$   
108  $CO_2$  values, and induced a higher ventilatory response, along a wide range of running  
109 intensities (from low to severe exercise domains). A 30% jaw protrusion seems to be  
110 sufficient to improve respiratory responses at submaximal exercise intensities, with  
111 the 50% protrusion being more favorable at higher exercise demands. When the  
112 protruding splints were worn, the lower limb running pattern was also modified, even  
113 if this effect was not clear for the angular variables. These physiological and  
114 kinematical outcomes show a positive influence of wearing protruding splints on  
115 performance at submaximal and maximal aerobic exercise intensities.

116 The protruding splints reduced the exercise energy expenditure and cost by  
117 decreasing the  $\dot{V}O_2$  at the same running velocity, concurrently with decreased  $\dot{V}CO_2$   
118 and increased ventilation and respiratory frequency. The differences between 30 and  
119 50% splints were clearer for the intensities above the AnT, probably related to the  
120 increasing importance of the respiratory system at higher exercise intensities.<sup>3</sup> These  
121 findings are similar to those previously reported where lower  $\dot{V}O_2$ <sup>3,7</sup> and  
122 hyperventilatory<sup>2,3</sup> responses were observed in subjects wearing intraoral splints or  
123 by unloading the respiratory muscle work during exercise. Taken together, these data  
124 support the hypothesis that placing the jaw forward increases the airflow and  
125 decreases the work of breathing. In contrast, previous studies reported little effects  
126 on gas-exchange<sup>8</sup> or even higher  $\dot{V}O_2$  values<sup>4</sup> when wearing occlusal or jaw  
127 forwarding splints. Differences between studies are most likely related to variations  
128 in the methodological assessment or, eventually, differences in splint design.

129 When the jaw was placed in more forward position, shorter contact times and stride  
130 lengths, as well as higher stride rates were observed. These effects are consistent with  
131 lower energy demand of locomotion and center of mass vertical excursion, indicative  
132 of more economical running.<sup>9,10</sup> Reductions in the degree of knee flexion are also  
133 related to running performance improvements<sup>10,11</sup> and a higher protrusion with the  
134 50% splint had a positive contribution across all running stages. Small changes in  
135 running patterns have been reported when different occlusal splints were worn<sup>12</sup> and,  
136 consequently, when the vertical dimension of occlusion was increased. However, it  
137 is difficult to justify why the 30% splint yielded different knee angular kinematics  
138 comparing to the 50% splint despite both splints providing the same degree of vertical  
139 dimension of occlusion.

## 140 Practical applications

141 The possibility of better supporting the high ventilatory demands by decreasing the  
142 airway resistance and the respiratory work when wearing a protruding splint would  
143 be of great interest for the sporting community. We investigated the biophysical  
144 effects of different protruded splints across a wide range of running intensities, with  
145 this being the first study to clarify and compare different protrusion ranges. We  
146 acknowledge the limitations of a case study design and the importance of studying  
147 the effects of protruding splints in larger cohort of runners. Since it is possible that a  
148 protruding splint might be more effective for subjects with narrow airways or, even,  
149 at certain environments, studying individual athletes in a case-by-case approach  
150 should not be discounted.

## 151 Conclusions

152 The outcomes of this case study support the assertion that protruding splints can have  
153 a positive impact on running performance. Placing the jaw forward enhanced the  
154 ventilatory response to exercise, with higher protrusion seeming to be better at higher  
155 intensities. Running kinematics were also improved when using an intraoral  
156 protruding splint device.

### 157 **Acknowledgments**

158 We acknowledge the Portuguese Foundation for Science and Technology, I.P. (FCT)  
159 and the European Union (EU) for the PhD individual grant (2020.05012.BD) to the  
160 lead author.

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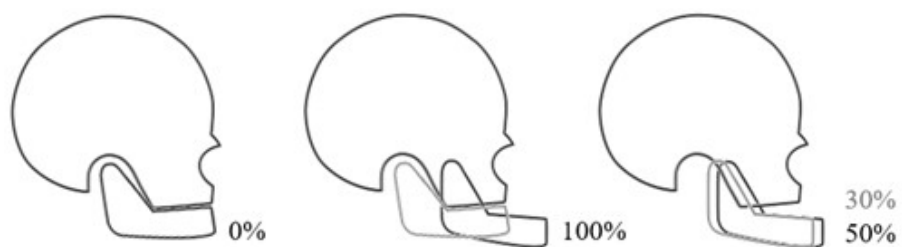


Figure 1 – Antero-posterior lower jaw position at different mandibular protrusions: 0% (without protrusion), 100% (absolute range of maximal protrusion) and 30 and 50% of the absolute range of maximal protrusion (left, center and right panels, respectively).

146x45mm (96 x 96 DPI)



Table 1. Physiological assessment across the incremental running protocol. The three intraoral mandibular splints assessed where placebo (0% advancement), 30 and 50% advancement of the jaw's maximum protrusion. Treadmill running velocity (v).

	Stage	1	2	3	4	5	6	7
	v (km·h <sup>-1</sup> )	11	12	13	14	15	16	17
Oxygen consumption (ml·kg <sup>-1</sup> ·min <sup>-1</sup> )	Placebo	40.1 (1.4) <sup>*†</sup>	44.4 (0.2) <sup>*†</sup>	45.0 (0.6) <sup>*†</sup>	47.1 (1.0) <sup>*†</sup>	52.3 (0.9) <sup>*†</sup>	53.1 (0.8) <sup>*†</sup>	56.1 (1.1) <sup>*†</sup>
	30%	34.9 (1.2)	39.3 (1.0)	43.2 (0.9)	46.0 (0.5) <sup>†</sup>	49.4 (0.8) <sup>†</sup>	52.0 (1.0) <sup>†</sup>	54.5 (1.2) <sup>†</sup>
	50%	36.3 (1.0)	38.6 (0.6)	42.0 (1.7)	44.5 (1.5)	46.6 (1.3)	49.9 (0.7)	52.4 (0.8)
Carbon dioxide production (ml·kg <sup>-1</sup> ·min <sup>-1</sup> )	Placebo	32.8 (0.9) <sup>*†</sup>	38.9 (0.4) <sup>*†</sup>	39.3 (0.7) <sup>†</sup>	42.9 (0.9) <sup>†</sup>	50.0 (1.1) <sup>*†</sup>	54.0 (1.0) <sup>*†</sup>	56.3 (1.1) <sup>†</sup>
	30%	30.3 (0.7)	34.5 (0.7)	40.2 (1.1) <sup>†</sup>	43.3 (1.1) <sup>†</sup>	48.8 (0.8) <sup>†</sup>	52.5 (1.7) <sup>†</sup>	56.8 (0.8) <sup>†</sup>
	50%	29.9 (0.9)	35.2 (0.5)	37.8 (1.0)	41.1 (1.3)	44.5 (1.3)	50.7 (1.2)	53.5 (1.2)
Ventilation (L·min <sup>-1</sup> )	Placebo	63.5 (1.7)	70.9 (1.0) <sup>†</sup>	73.8 (1.6) <sup>*†</sup>	86.6 (2.4) <sup>*†</sup>	103.9 (1.2)	113.4 (2.2) <sup>*†</sup>	124.9 (1.6) <sup>†</sup>
	30%	65.4 (2.1)	71.0 (2.3) <sup>†</sup>	83.0 (2.2)	94.0 (3.3)	103.7 (1.7)	117.8 (1.5) <sup>†</sup>	125.6 (2.5)
	50%	64.3 (1.1)	75.2 (2.0)	81.9 (1.3)	91.7 (2.7)	102.7 (1.4)	124.0 (1.3)	127.0 (1.6)
Respiratory frequency (b·min <sup>-1</sup> )	Placebo	40 (2) <sup>*†</sup>	42 (2) <sup>*†</sup>	44 (2) <sup>*†</sup>	52 (2) <sup>*†</sup>	55 (2)	58 (1) <sup>*†</sup>	60 (1) <sup>*†</sup>
	30%	45 (2)	48 (1)	51 (1)	56 (2)	57 (2)	61 (2)	64 (1)
	50%	43 (1)	47 (1)	51 (1)	55 (1)	56 (2)	61 (2)	64 (1)
Energy expenditure (ml·kg <sup>-1</sup> ·min <sup>-1</sup> )	Placebo	33.0	39.4	40.0	49.3	54.8	67.3	69.1
	30%	31.1	34.3	39.1	49.4	54.6	62.9	64.5
	50%	28.6	33.6	37	46.7	53.9	59.6	60.9

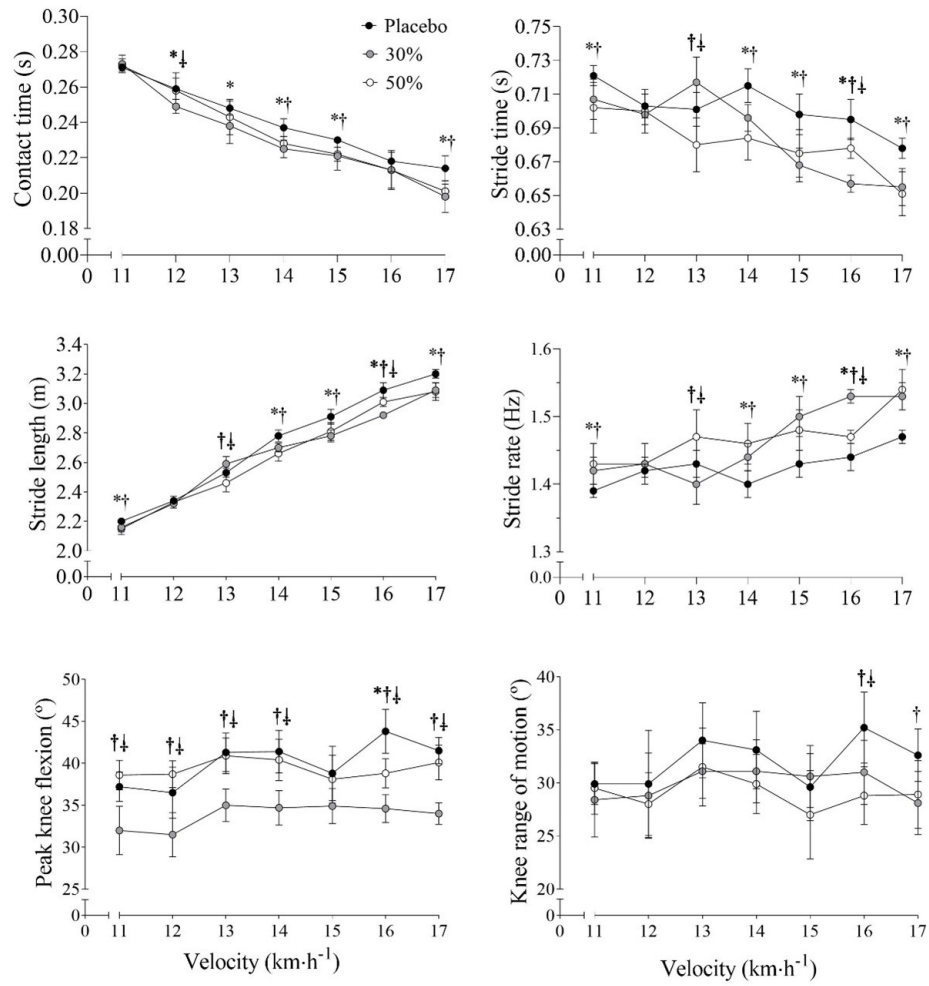


Figure 2 – Running linear and knee angular kinematics for 0 (placebo), 30 and 50% intraoral splint devices. \*, † and □ indicates differences between placebo and 30 and 50%, and between 30 and 50% (respectively).

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