# Fabrication of low cost and low impact RH and temperature sensors for the Internet of Environmental-Friendly Things

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10 Abstract- Given the increasing number of connected devices as a consequence of the Internet 11 of Things (IoT) revolution, the issue of the removal and recycling of electronics is becoming 12 more and more urgent. In this context, biodegradable electronics is expected to be one of the 13 biggest technological revolutions to tackle this problem. Following this direction, in this work 14 we present the fabrication and characterization of temperature and humidity sensors based on 15 biodegradable materials with the goal of making their removal easier as well as reducing their 16 environmental impact. In particular, these multi-sensing devices were fabricated following a 17 screen-printing process using a carbon-based paste and a conjugated polymer, both on paper 18 and on a water soluble substrate. The results are more than promising and show how with our 19 biodegradable sensors it is possible to obtain a sensitivity of 1 dec/20% RH to moisture content 20 and around 0.04%/°C sensitivity to temperature. It is demonstrated that the simplicity and 21 flexibility of the fabrication approach followed in this work paves the way to a set of new "green" 22 IoT nodes that could be extended to wide range of sensing applications.

## 23 Keywords: carbon; humidity; paper; PVA; PEDOT:PSS; screen-printing; temperature

## 24 **1. Introduction**

Sensing technologies are one of the key fields in both consumer electronics and industrial environment. Today we are measuring everything; sensors are in cars, buildings, cell phones, watches, and many other things of our daily life. Thus, this trend towards an ubiquitous sensing has made that the research and development in this field becomes particularly interesting.

Humidity sensors are among the most studied in this area since they play a key role in several
areas, such as agriculture, food industry or healthcare (e.g., pharmaceutical & bio-tech

fabrication) [1], [2]. Humidity sensors are usually capacitive or resistive and, although there are further variations, they differ from others mainly in their preciseness, time response, size and costs [3]. However, given the circumstances imposed by the new technological applications, further aspects are becoming of special interest for their development, such as flexibility, biocompatibility or easy disposability [4]–[6]. This has led the novel fabrication methods to be focused not only on a highly scalable and economic production of devices, but also on their biodegradability in order to minimize, or even eliminate, their impact on the environment [7].

Printed sensors step exactly in this demand, as they allow the fabrication of cost-effective sensors based on fully biodegradable conductive pastes, sensitive materials and substrates [8], [9]. Therefore, several printable and organic materials have been proposed in this direction, such as conjugated polymers [9], graphene-based materials [10]–[12] and carbon-based pastes [13]. In the same way, different flexible substrates have also been used to deposit these materials, including paper [14]–[16] or liquid crystal polymers [17], [18], among others [19], [20].

44 Many of these materials and substrates has been already studied to develop temperature and 45 humidity sensors, however, most of the implementations proposed in the literature resort to 46 non-biodegradable materials to develop some elements of the final devices. For instance, Khan 47 et al. presented a printed humidity sensor based on an egg albumin sensitive layer, but using 48 silver electrodes on a PET substrate [21]. This approach was also followed in [22] and [12] 49 using graphene oxide as sensitive layer and, in general, it can be found in many other works 50 with different kind of materials [21], [23], [24]. Alternatively, Alrammouz et al. proposed a 51 capacitive humidity sensor based on self-assembled graphene oxide sheets on a paper substrate, 52 but with the drawback of using electrodes made of aluminum [25].

53 Within this context, in this work we present the fabrication and characterization of flexible 54 humidity and temperature sensors by means of printing techniques and biodegradable materials 55 (for both electrode and substrate) that are fully compatible with a cost-effective fabrication of 56 eco-friendly devices. For that, a simple screen-printing process was used, demonstrating the 57 feasibility of this approach through the combination of different conductive pastes and 58 substrates. On one hand, we used standard paper as substrate since, in addition to being 59 compatible with printing techniques and providing flexibility, its hydrophilic nature makes it a perfect candidate to act as a sensing material in RH sensors [26]-[28]. On the other hand, poly-60 61 vinyl alcohol (PVA) films were also used for this purpose, given that the dielectric and 62 conductive properties of this hygroscopic polymer change when the hydroxyl groups (O-H) of its structure interact with the water molecules [29]. These two substrates were used to print on
them different electrodes configurations also using fully biodegradable conductive materials,
specifically poly(3,4-ethylenedioxythiophene) polystyrene sulfonate (PEDOT:PSS) and a
carbon-based paste. Each possible combination of these two conductive pastes and substrate
materials was fabricated and characterized.

The manuscript is structured as follows: following this introduction, Section 2 summarizes the materials used for the fabrication of the sensors, together with the methodologies followed for their characterization. Section 3 presents the results of the temperature and humidity sensors fabricated, as well as a hybrid configuration to monitor both temperature and humidity on the same device. Finally, the main conclusions are drawn in Section 4.

#### 73 **2. Experimental Section**

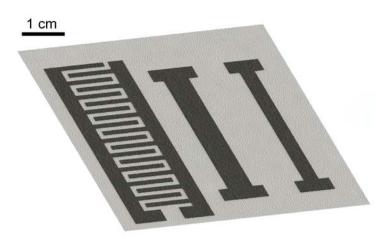
#### 74 **2.1. Materials**

75 Two conductive inks were used for the fabrication of the printed sensors, poly(3,4-76 ethylenedioxythiophene)-poly(styrenesulfonate) (PEDOT:PSS) and a commercial carbon-77 based paste, both of them providing flexibility and biodegradability. PEDOT:PSS at a weight 78 content of 1.3 wt.% (viscosity: >14000 mPa.s) was acquired from Sigma Aldrich (St. Louis, 79 MO, USA) [30], while the Loctite ECI 8001 E&C carbon-based paste (viscosity: 6500 mPa.s) 80 was provided by Henkel AG (Düsseldorf, Germany) [31]. These pastes were printed on three 81 different substrates: standard paper (DIN ISO 9706, 80g/m<sup>2</sup>) [32], polyvinyl alcohol (PVA) 82 films from Wagner Polymertechnik GmbH, and polyethylene terephthalate (PET) foils from 83 DuPont (product name: Melinex® 506, Wilmington, DE, USA) [33]. This latter only for 84 comparison and control since it is not biodegradable.

#### 85 **2.2. Devices Fabrication**

86 A capacitive Interdigitated Electrode (IDE) structure was considered for the RH monitoring 87 devices. Given that the dependence of the dielectric constant of the substrates with respect to 88 the RH, the capacitance of these structures is also subject to the level of RH [34]. The advantage 89 of the IDE layout lays in the simplicity of its geometry, and therefore, its easy application via 90 printing on the flexible substrates [35]. After optimizing the four combination of pastes and 91 substrates by printing lines of several widths, the combination carbon on PVA-L limited the 92 resolution of our patterns with 800 µm as minimal reproducible dimension. The IDE structure used in work (Figure 1) has 10 fingers per electrode with a distance between consecutive fingers 93

94 and width of 1 mm. These dimensions are large enough to minimize the possible effects on the 95 capacitance as a consequence of the paste spreading over the substrate after the screen-printing 96 process. Moreover, given that the resistivity of both of the conductive pastes used is 97 temperature-dependent [31], [36], we opted for a resistive sensor for the temperature monitoring 98 which consisted of a simple line with a length of 5 cm. In addition, in order study the change in 99 resistance with respect to the temperature (sensitivity and hysteresis) at different average 100 resistances, we tested two different lines widths (3 mm and 5 mm), as it is shown in Figure 1.



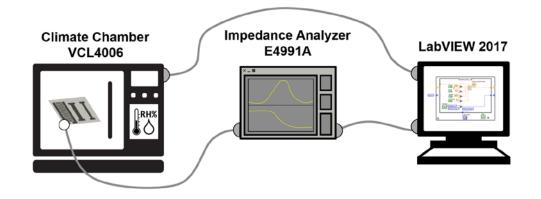
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Figure 1. Left: Capacitive IDE layout. Right: Resistive line layouts with the same length (5 cm) and different
 widths (5 mm and 3 mm).

104 These layouts were screen-printed with the different pastes on the different substrates with a 105 manual screen-printer (FLAT-DX200, from Siebdruck-Versand, Magdeburg, Germany). 106 Before printing, the PET substrate was washed using deionized water and ethanol with the 107 assistance of ultrasonic treatment in order to remove the impurities on the surface [37]. 108 Moreover, pressurized air was applied to the paper substrate with the same purpose, whereas 109 no cleaning process was carried out for the PVA films. No pretreatment was needed to screen 110 printing the pastes on any of the substrates. The mesh used in this work was a 120 Threads per 111 cm (T/cm) polyester mesh with a thickness of 65  $\mu$ m, a thread diameter of 40  $\mu$ m and an opening 112 width of 47 µm which, according to the manufacturer, results in a theoretical wet film thickness 113 of  $t_{\text{theo}} = 19.5 \,\mu\text{m}$ . After printing, the samples were dried using a UF55 oven (from Memmert, Schwabach, Germany) at 80 °C in order to avoid the degradation of the substrates. We also 114 115 considered two different curing times, 30 min and 60 min, to evaluate the influence of the drying 116 process in the conductivity of the screen-printed patterns.

#### 117 **2.3. Characterization**

- 118 The sheet resistance of the conductive layers was measured using a four-point probe head from
- 119 Jandel (Leighton Buzzard, UK) connected to a source measuring unit (Keysight B2901A,
- 120 Beaverton, OR, USA). The thickness of the samples was acquired using a DekTak XT contact
- 121 profilometer (from Bruker Corporation, Billerica, MA, USA).
- The characterization of the sensors under different environmental conditions (temperature and humidity) was performed using the setup shown in Figure 2. The sensors were connected to an impedance analyzer E4991A using a 42941A impedance probe kit (both from Keysight Technologies, Inc., CA, USA). Afterwards, each connected sensor was placed into a climate chamber VCL4006 (from Vötsch Industrietechnik GmbH, Balingen, Germany) and its impedance was measured from 1 kHz to 10 MHz under different values of temperature and humidity. The whole measurement setup was automatized using LabVIEW 2017 (from
- 129 National Instruments Corporation, TX, USA).



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Figure 2. Characterization setup for humidity and temperature sensors.

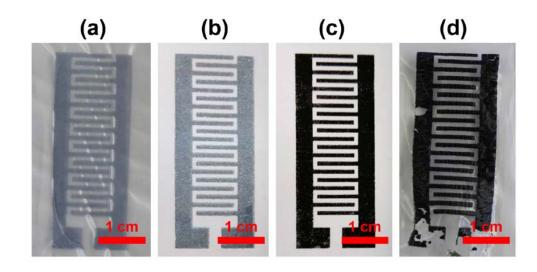
The humidity sensors were tested as a function of both variating humidity and temperature. Firstly, the humidity sensors were characterized ranging the relative humidity level from 20%RH to 70%RH and vice versa at a temperature of 40 °C. RH was changed in steps of 10%RH every 30 min to ensure the uniformity of RH value in the whole chamber's volume. Secondly, both sensors (resistive and capacitive) were characterized as a function of the temperature. For that, it was ranged from 15 °C to 75 °C and vice versa at a fixed 60%RH. In this case, the temperature was varied in steps of 5 °C every 20 min.

#### 139 **3. Results and Discussion**

Throughout this section, we show the results obtained for the characterization of both humidity and temperature sensors fabricated with the biodegradable carbon-based and PEDOT:PSS pastes on both paper and PVA films. The results are also compared with respect to those obtained using PET as substrate of reference.

#### 144 **3.1. Physical Characterization**

145 All the fully-biodegradable RH sensors fabricated in this work are shown in Figure 3. After 146 visual inspection, it can be clearly observed that all inks were properly transferred to the 147 substrates, except for the carbon-based paste on the PVA substrate (Figure 3d). In that case, the 148 printing of the carbon paste (with a thickness of  $10 \pm 1.2 \,\mu$ m) on the thin PVA substrate (30 149 µm) produces a non-flexible device. Thus, when this device is bent, cracks appear on the whole 150 carbon layer surface. However, this does not happen on the paper substrate, whose surface roughness and greater thickness (~100 µm) enhance the adhesion of the carbon-paste (Figure 151 152 3c). On the contrary, the PEDOT:PSS layer, which is thinner  $(2 \pm 0.3 \,\mu\text{m})$ , presents a good 153 adhesion and flexibility on both paper and PVA substrates.



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Figure 3. Real view of the screen-printed sensors: (a) PEDOT:PSS on PVA, (b) PEDOT:PSS on paper, (c) carbon based paste on paper and (d) carbon-based paste on PVA. Scale bars: 1 cm.

157 The sheet resistances of each one of these patterns are presented in Table 1 for the different 158 curing conditions. These values were obtained at ambient conditions, whereas errors were 159 calculated as the standard deviation of five different samples. As seen, any substantial variation 160 was observed when increasing the curing time. These values are also in accordance with respect 161 to the obtained in other works, both for PEDOT:PSS [38]–[40] and for carbon-based pastes

162 [41].

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**Table 1.** Sheet resistance values for the different pastes and substrates under different curing conditions.

Paste	Substrate	Sheet Resistance ( $k\Omega/sq.$ )	Sheet Resistance ( $k\Omega/sq.$ )	
raste	Substrate	(curing: 30 min at 80 °C)	(curing: 60 min at 80 °C)	
Carban	Paper	$3.84\pm0.86$	$3.73\pm0.84$	
Carbon	PVA	$3.89\pm0.93$	$3.85\pm0.93$	
PEDOT:PSS	Paper	$1.20\pm0.13$	$1.09\pm0.08$	
PEDOT:PSS	PVA	$1.21\pm0.16$	$1.09 \pm 0.09$	

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#### 168 **3.2. Characterization in relative humidity**

Firstly, we characterized the impedance of the capacitive humidity sensors as a function of the RH. The results of these experiments are shown in Figure 4 for the PEDOT:PSS IDEs and in Figure 5 for the carbon-based ones. Reference calibration curves on PET can be found in supplementary Figure S1 and Figure S2, respectively.

173 On one side, the impedance of both carbon paste and PEDOT:PSS on PET shows no 174 dependence on RH at any of the studied frequencies. In that case, the modulus and phase of the 175 impedance remain almost constant for the different values of RH and decrease as the frequency 176 increases. In the case of the phase, the decrease is less abrupt and, as capacitive structure, it is 177 around -90° [42]. On the other side, it can be seen in Figure 4 that the same capacitive structure behaves differently on the other substrates. At low RH values, both on paper and PVA, the 178 179 PEDOT:PSS structures behave as a capacitor (phase close to -90°). However, as RH increases, 180 the phase decreases indicating an increase in the capacitor dissipation factor. This phenomenon 181 can be related to an increase in the polymer conductivity as a consequence of the moisture 182 accumulation on the sensing layer (i.e., the substrate), hence causing the apparition of electrical

- 183 paths between electrodes. As a result of this, at high RH levels the devices start to behave more
- 184 like a resistor (phase closer to 0°) than like a capacitor [42].

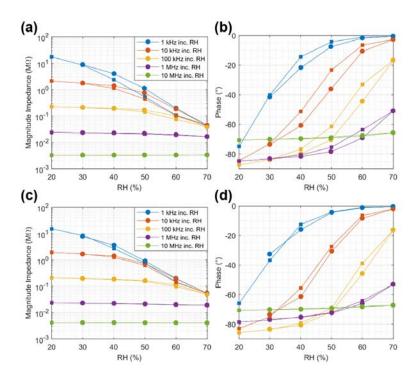
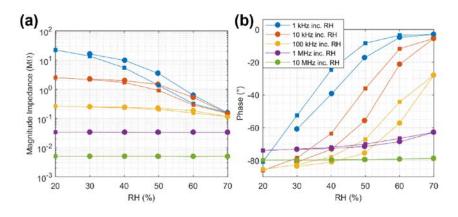


Figure 4. Impedance of the PEDOT:PSS IDEs on paper (magnitude: (a), phase: (b)) and on PVA (magnitude: (c), phase: (d)).



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Figure 5. Impedance of the carbon IDEs on paper (magnitude: (a), phase: (b)).

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Moreover, this behavior is similar to that obtained for the carbon-based IDEs on paper, as shown in Figure 5, which supports the theory that dependence with respect to the RH arises mainly from the properties of the sensing layer [43]. Finally, Figure S3 shows the results obtained for the the carbon- based paste on PVA, which demonstrates the non-viability of this combination for screen-printing (as it was shown in Section 3.1).

196 In general, in all cases a sensitivity as high as 1 dec/20%RH can be reproducibly achieved. In 197 all the analyzed combination of materials, the impedance changes abruptly from 20 to 60% RH 198 and then its responses is saturated. This behaviour is particularly significant up to 100 kHz. At 199 low RH values, the devices are mainly capacitive (phase <80°) and when RH increases, their 200 phases decrease, achieving phases above -10° at 60% RH (mainly resistive). However, there are 201 differences related to the hysteresis of the sensors, the lowest value (below 3%) is found for 202 PEDOT:PSS IDES on PVA, followed by PEDOT:PSS on paper (5%). In general, as it can be 203 seen in Figure 4 and Figure 5, the paper substrate results in a higher hysteresis than the case of 204 the PVA substrate.

Regarding the dynamic response of the sensors, we define the response time as  $t = \tau$ , which corresponds to the 63% of the maximum value of magnitude reached at equilibrium (for every increasing step of RH). Table 2 summarizes the response time for each one of the analysed devices.

#### 209

Table 2. Time response for RH

Substrate	Time response of PEDOT:PSS IDES (min)	Time response of Carbon IDES (min)
PVA	5.8	6.5
Paper	4.6	4.8

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#### 211 **3.3. Characterization in Temperature**

212 As it was already introduced, the resistivity of both PEDOT:PSS and carbon-based pastes used 213 in this work is temperature-dependent. In the case of the PEDOT:PSS, it exhibits a Negative 214 Temperature Coefficient (NTC) [36], [44], whereas the Loctite ECI 8001 E&C paste is a 215 Positive Temperature Coefficient (PTC) ink [31]. On this basis, we characterized the impedance 216 of the resistive patterns as a function of the temperature on a paper substrate. Looking at the 217 behavior of single lines on paper using the same conductive materials (Fig. 6), we found that 218 PEDOT:PSS showed a relative linear response at 1 kHz in the temperature range analyzed, as 219 it was also demonstrated in other works [45], [46]. These sensors exhibited a sensitivity of 220 around 0.04%/°C and 0.03%/°C (considering the relative resistance change as output variable) 221 for the 3 mm and 5 mm lines width, respectively. Contrary to this, carbon lines exhibited a quite 222 linear response at low temperatures, but surpassing the ~50 °C their resistivity presented a sharp 223 step response. It can be also seen that the response of the carbon-based paste presents a higher

hysteresis than the PEDOT:PSS paste. These two effect are in accordance with the dataprovided by the manufacturer [31].

For these structures, the sensitivity can be estimated as 3%/°C, which is significantly high enough to be easy detectable with any low-cost measurement equipment. Furthermore, the results obtained for the lines with 5 mm of width (supplementary Figure S4) showed that, while the temperature response and hysteresis of the PEDOT:PSS patterns does not suffer significant changes, the hysteresis presented by the carbon-based paste is reduced as a consequence of the overall reduction of the pattern resistance.

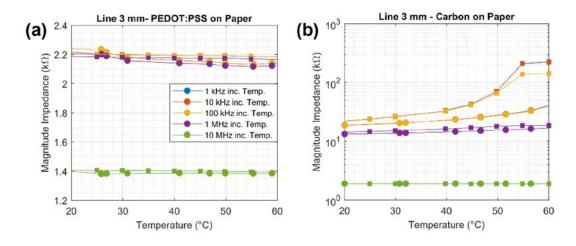


Figure 6. Impedance vs. temperature at different working frequencies of lines on paper made of PEDOT:PSSand Carbon with width of 3 mm.

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235 Regarding the dynamic response of the sensors and following the same definition as the one

employed for RH, Table 3 depicts the response time for each sensor characterized.

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 Table 3. Time response for Temperature

Substrate	Time response of PEDOT:PSS IDES (min)	Time response of Carbon IDES (min)
PVA	3.9	3.3
Paper	4.5	3.8

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### **3.4.** Comparison with similar sensors in the literature

In this section, we compare the sensors proposed in this work with other fully biodegradable sensors presented in the literature. The comparison was made in terms of type of sensor, materials, fabrication process, area and sensitivity to the variable to monitor (temperature or 243 humidity), as presented in Table 4. In recent years, novel approaches on carbon nanotubes 244 (CNTs) in their various forms, single-wallet and multi-wallet (SWCNTs, MWCNTs), are 245 positioning this material among the most promising materials for the development of 246 biodegradable sensors [47]. For instance, Liakos et al. [48] and Zhu et al. [49] used this 247 conductive organic material to fabricate humidity sensors on different biodegradable substrates, 248 achieving a quite similar sensitivity to humidity changes. However, although these sensors also 249 provide interesting features such as flexibility, their fabrication processes do not allow to pattern 250 surface of the substrates in order to optimize the sensing area. Contrary to this, printing 251 techniques are able to transfer different kind of layouts on the substrates, such as the capacitive 252 structures presented in this work, which allows to enhance the sensitivity of humidity sensors 253 more than two orders of magnitude. In addition, some of the presented processes are not suitable 254 for a large-scale and cost-effective production of devices, as it is de case of the one presented 255 in [49].



#### Table 4. Comparison with other biodegradable sensors.

Defenses	Comeran Train	Electrode and	Estudios Duo com	Area	Sensitivity
Reference Sensor Typ		Substrate Materials	Fabrication Process	(cm <sup>2</sup> )	(∆ Z /°C or ∆ Z /%RH )
Salvatore <i>et al.</i> [50]	Temperature	Mg/EcoFlex	UV lithography / etching	7	70 Ω/°C
Yi <i>et al.</i> [51]	Temperature	Zn/Galactomannan	Drop Casting	~0.5	5 Ω/°C
Liakos <i>et</i> <i>al</i> . [48]	Humidity	SWCNT, Sodium alginate, CaCl2	Immersion/Coating	-	1210 Ω/%RH @ 1kHz
Zhu <i>et al.</i> [49]	Humidity	Cellulose Nanofibers, CNTs	Vacuum filtration	0.5	~1307 Ω/%RH @ DC voltage
Syrový <i>et</i> <i>al.</i> [52]	Humidity	Carbon Paste Cellulose nanofibril	Screen-Printing	1	Up to 122 kΩ/%RH @ 1kHz
Liu <i>et al.</i> [53]	Temperature	Laser-Induced Graphene (LIG)/Starch Film	Laser-Patterning and Transferring	-	~1.2 kΩ/°C
Barras <i>et al.</i> [54]	Humidity	Carbon Filaments and carboxymethyl cellulose on Paper	Screen-printing	0.7	~2.6 kΩ/%RH @ DC voltage
		PEDOT:PSS on Paper			217.2 kΩ/%RH @ 1kHz
This work	Humidity	PEDOT:PSS on PVA	Screen-Printing	4	207 kΩ/%RH @ 1kHz
		Carbon Paste on Paper	-		204 kΩ/%RH @ 1kHz

	PEDOT:PSS on Paper			25 Ω/°C @ 10kHz
Temperature		Screen-Printing	1.5	
	Carbon Paste on Paper			75 Ω/°C

258 In the case of biodegradable temperature sensors, authors like Salvatore *et al.* [50] and Yi *et al.* 259 [51] also opted for the pattering of resistive layouts on biodegradable substrates; one of them following a UV lithography and etching process, after which the pattern is transferred to the 260 261 substrate (which is a similar process to the one followed in the LIG-based sensor presented by 262 Liu *et al.* [53]); and the other following a mask-aided drop casting method. It can be seen that 263 the sensitivities of the temperature sensors presented in this work are higher than that obtained 264 with the Mg-based and Zn-based sensors, even with smaller areas (e.g., when compare the 265 carbon-based sensor with respect to the Mg-based one). Regarding printed sensors, although 266 there are numerous screen-printed as well as inkjet-printed sensors reported in the literature, 267 most of them are based on non-biodegradable materials (either the electrodes or even both 268 electrodes and substrates). Among the few fully biodegradable sensors that can be found are 269 the screen-printing approaches presented by Syrový et al. [52] and Barras et al. [54], which 270 demonstrate the trend towards the use of carbon materials on cellulose-based substrates for the 271 fabrication of fully biodegradable and printed sensors.

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## 273 **3.5.Characterization as Hybrid Sensors**

274 Based on the results obtained for both RH and temperature sensors, the devices fabricated could 275 be successfully employed in a hybrid sensor, where the RH is extracted by measuring the 276 impedance between the terminals of IDE structure, and the temperature through one of the 277 junctions of the IDE structure, i.e., the line that links all fingers of one IDE terminal [55]. To 278 exemplify this concept, in Figure 7 we show a comparison between the impedance of a carbon-279 based line of 3 mm of width and the impedance of a carbon-based IDE structure on the same 280 substrate (paper). These results show how at 1 kHz and 10 kHz the combination of the two 281 measurements, at the IDE terminals and at the line ends, would provide sufficient data to isolate 282 the effects of temperature and humidity, resulting in a biodegradable, compact, simple and cost-283 effective multi-sensing method.

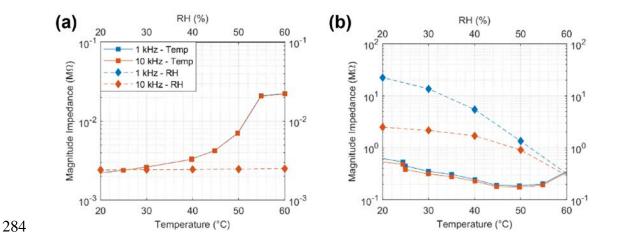


Figure 7. Impedance as a function of temperature and RH for a carbon-based line with 3 mm of width (a) and a carbon-based
 IDE structure (b), both on paper.

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#### **4.** Conclusions

289 With this contribution, we intend to shift the focus of research in printed electronics and sensors 290 towards a real sustainability of printed Internet of Things nodes. For this reason, we designed, 291 fabricated and characterized a set of different sensors with biodegradable materials (both 292 conductive materials and insulating substrates), in order to measure the temperature and 293 humidity content in the environment. Our low-cost, sustainable and high throughput method 294 allowed us to produce multi-sensing devices made of conductive polymers and a carbon-based 295 paste on both paper and PVA substrates. The performances of these sensors are remarkable and 296 detectable with low-cost equipment (0.04% change in relative resistance per degree Celsius, 1 297 dec change in impedance per 20% RH). This factor, in combination with the facile production 298 method and the significantly reduced environmental impact, makes this new class of sensors 299 promising candidates for a sustainable development of sensors within the Internet of Everything 300 paradigm.

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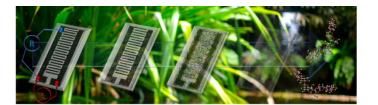
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- 492 Fabrication and characterization of fully printed biodegradable sensors for humidity and
- 493 temperature sensing. These sensors will contribute enormously to pave the way to more
  494 cost-effective and environmental friendly devices.
- 495 Keywords: carbon; humidity; paper; PVA; PEDOT:PSS; screen-printing; temperature
- 496 Aniello Falco, Philipp S. Sackenheim, Francisco J. Romero, Markus Becherer, Paolo Lugli,
- 497 José F. Salmeron, Almudena Rivadeneyra<sup>\*</sup>
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