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# BIOMATERIALS

# Tissue engineering strategies for the treatment of tendon injuries

A SYSTEMATIC REVIEW AND META-ANALYSIS OF ANIMAL MODELS

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 Recently, the field of tissue engineering has made numerous advances towards achieving artificial tendon substitutes with excellent mechanical and histological properties, and has had some promising experimental results. The purpose of this systematic review is to assess the efficacy of tissue engineering in the treatment of tendon injuries.

# University of Granada, Methods

We searched MEDLINE, Embase, and the Cochrane Library for the time period 1999 to 2016 for trials investigating tissue engineering used to improve tendon healing in animal models. The studies were screened for inclusion based on randomization, controls, and reported measurable outcomes. The RevMan software package was used for the meta-analysis.

## Results

A total of 388 references were retrieved and 35 studies were included in this systematic review. The different biomaterials developed were analyzed and we found that they improve the biomechanical and histological characteristics of the repaired tendon. At meta-analysis, despite a high heterogeneity, it revealed a statistically significant effect in favour of the maximum load, the maximum stress, and the Young's modulus between experimental and control groups. In the forest plot, the diamond was on the right side of the vertical line and did not intersect with the line, favouring experimental groups.

#### Conclusions

This review of the literature demonstrates the heterogeneity in the tendon tissue engineering literature. Several biomaterials have been developed and have been shown to enhance tendon healing and regeneration with improved outcomes.

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Keywords: Tissue engineering, Tendon injury, Cell-based therapies, Tendon healing, Biomaterials, Review

#### **Article focus**

- Tissue engineering has emerged as an interesting alternative in regenerative medicine thanks to its development in recent years.
- Researchers have produced bioartificial substitutes that, by combining cells, biomaterials, and growth factors, restore the function of damaged organs.
- The objective of this study was to assess the efficacy of tissue engineering in the treatment of tendon injuries in animal models by systematically reviewing the scientific literature.

#### **Key messages**

Complete regeneration of the tendon after injury is never achieved and the

surgical treatment of these lesions have several limitations.

The use of tissue engineering techniques can accelerate the healing process and produce biomechanical behaviour comparable to that of native tendons.

#### **Strengths and limitations**

- No previous reviews have produced a meta-analysis of biomechanical results of tissue engineering for the treatment of tendon injuries in animal models.
- The included studies were heterogeneous in several ways, including the animal models used and tendon models used.

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#### Introduction

Most large tendons, such as the Achilles tendon, patellar tendon, rotator cuff, or forearm extensors, among others, are vulnerable to overuse, which can lead to pathological changes in the tendon that cause tendinopathy. This pathology is common among athletes and workers, being the main reason for musculoskeletal consult to the general practitioner (about 30%) and accounting for 17% of first consultations to the orthopedic surgeon.<sup>1</sup> Acute tendon injury includes partial or complete rupture, altering the continuity of the tendon and causing loss of movement. It is followed by a natural healing process but is less efficient than in other components of the musculoskeletal system. Acute and chronic injuries are facilitated by intrinsic and extrinsic factors. For example, degeneration of collagen and alteration of the orientation of its fibres have been shown in the histology of ruptures of the Achilles tendons.<sup>2</sup>

Complete regeneration of the tendon after injury is never achieved. The characteristic response is fibroplasia and the tissue that replaces the defect remains hypercellular with thinner collagen fibres. In tendons with tendinopathy or ruptures, there is a lower proportion of type I collagen and an increase in the amount of type III collagen, which reduces the mechanical resistance because this type of collagen has less crosslinking than type I.<sup>3</sup>

Currently, tendinous repair includes the use of autografts and tendinous transfers because allografts lose their biomechanical properties during the process of sterilization. In this context, tissue engineering emerged as a promising alternative in regenerative medicine, including tendinous repair. Tissue engineering is a multidisciplinary discipline that, through the rational combination of cells, biomaterials, and growth factors, allows the generation of bioartificial substitutes to repair, replace, or even increase the function of damaged tissues or organs.<sup>4,5</sup>

At present, tissue engineering researchers are developing polymers and 3D bioartificial substitutes that accelerate the healing process with biomechanical behaviour comparable to that of native tendons. However, to date, the studies on tendon repair using animal models have not found an ideal biomaterial and 3D bioartificial substitute for this purpose.<sup>6</sup>

Because these experimental studies have shown favourable results for the use of tissue engineering in tendon injuries, an update of the current evidence is required. This study presents a systematic review and meta-analysis of the existing progress in tissue engineering combining stem cells, growth factors, and scaffolds to assess the efficacy of treating tendon injuries in animal models.

## **Materials and Methods**

**Search strategy.** PRISMA guidelines were followed for this systematic review.

MEDLINE, Embase, and the Cochrane Library were searched for articles published between 1999 and 2016 about the use of tissue engineering in tendon injuries. The keywords used to conduct the research were "tendon injuries" and "tissue engineering".

Two researchers (DGQ, IMM) reviewed all of the potential abstracts and full texts independently. If there was any disagreement, it was resolved by consultation with another researcher (AC).

**Article selection.** The studies were included if they investigated tissue engineering techniques (e.g. biomaterials, growth factors) for repairing a tendon lesion. Trials where required to have been conducted in animal models without restriction of specie. *Ex vivo* experimental studies were excluded. The *in vivo* studies that investigated biomechanical or histological outcomes by tissue engineering strategies in injured tendons were also included. Due to the nature of intervention, it was agreed trials without blinding design.

We excluded duplicated studies, review articles, case reports, editorials and studies that were not published in English and: which were not reported as full-text articles; which reported on a molecular or genetic level; which reported without a control group (e.g. normal tendons or tendons repaired with or without a tissue engineering approach); and experimental trials without an animal model of tendon injury.

**Quality assessment.** The ARRIVE Guidelines for reporting animal research were used to measure the methodological quality of all included studies.<sup>7</sup> This checklist of 20 items considers characteristics of animal used and the experimental, statistical, and analytical methods of each study. We set a low, medium, and high quality of the papers with a ARRIVE checklist of 12 or less, 13 to 15, and 16 or more respectively.

**Statistical analysis.** All analyses were performed using the RevMan software (version 5.0, The Cochrane Collaboration, Oxford, United Kingdom). Standard mean difference with 95% confidence interval (CI) was calculated. Heterogeneity between studies was examined using the I<sup>2</sup> statistical test. When the I<sup>2</sup> value was greater than 50%, we considered that heterogeneity was significant. A random effect model was chosen as the main analysis method. Funnel plots were used to check for the potential of publication bias. All the p-values were twosided; statistical significance was defined as p<0.05.

#### Results

**Literature search and study characteristics.** A total of 388 records were identified for abstract review after removal of duplicates. A total of 105 studies were excluded because of their focus on gene therapy, biomechanics, *ex vivo* experiments, or clinical studies. A total of 176 studies were not included due to their being review articles or discussions, and 20 records were excluded for not being published in English. Of the remaining 43 potential articles, two studies were excluded because the animal model did not include a tendon injury and three articles were excluded due to their focus on gene therapy,



Flowchart showing the selection process.

tendon-bone graft, and cell carriers, respectively (without animal model). A further three articles were excluded for being part of the same research.

Therefore, a total of 35 studies were included in this review, as reported in Figure 1. The selected articles are summarized in Supplementary table i. A total of 16 studies were included in the meta-analysis.

A total of 15 studies (42.9%) used rabbit models; the same number of trials used rat models. Two studies (5.7%) used hens. Pig, sheep, and dog animal models were used in one trial (2.9%) each. The tendons selected as lesion prototypes were: Achilles tendon (15, 42.9%); patellar tendon (seven, 20%); digital deep flexor tendon (six, 17.1%); supraspinatus tendon (three, 8.6%);

	Expe	Experimental			Control			Std. Mean Difference	Std. Mean Difference
Study or Subgroup	Mean	SD	Total	Mean	SD	Total	Weight	IV, Random, 95% CI	IV, Random, 95% CI
Awad 2003	118.3	42.3	8	38.2	18.7	8	8.6%	2.32 [0.97, 3.66]	*
Güngörmüs 2015	99.61	3.08	5	78.89	4.05	5	7.3%	5.20 [2.02, 8.38]	+
Juncosa A 2006	277.9	20	12	198	14.9	12	8.5%	4.37 [2.80, 5.95]	-
Juncosa B 2006	202.9	32.5	13	184.5	36	13	8.8%	0.52 [-0.26, 1.30]	•
Meimandi A 2013	28.33	2.19	10	4.56	1.92	10	6.7%	11.05 [7.13, 14.98]	
Meimandi B 2013	74.02	7.84	10	9.82	3.91	10	7.0%	9.93 [6.38, 13.47]	-
Moshiri A 2013	95.37	4.71	10	28.33	2.19	10	4.9%	17.48 [11.37, 23.59]	
Oryan A 2014	88.3	12.97	10	41 42	11.33	10	8.7%	1.83 [0.75, 2.91]	[
Oryan C 2012	120.01	0.07	10	41.42	5.77	10	6.0%	12 20 [9 62 17 00]	·
Organ D 2014	28 33	2 10	10	41.42	1.02	10	6.7%	11.05 [7.13.14.08]	
Shen 2010	68 5	18	5	65.7	10.3	5	8.7%	0 17 [-1 07 1 42]	•
Yokova 2012	111.9	9 4 3	8	44 3	3.67	8	6.9%	8 93 [5 24 12 63]	-
Zhao 2014	32.7	1	8	14.9	0.3	8	3.1%	22.80 [13.65, 31.95]	
		_	-			-			
Total (95% CI)			129			129	100.0%	6.82 [4.82, 8.83]	•
Heterogeneity: Tau <sup>2</sup> =	= 11.69; (	$Chi^2 = 1$	84.79,	df = 13	(P < 0.	00001)	; <b>I</b> <sup>2</sup> = 93%		
Test for overall effect	: Z = 6.6	6 (P < 0	.00001	.)					Favours [control] Favours [experimental]
									ratears [control] ratears [experimental]
Fig. 2a									
Eventual Control Std Very Difference Cod Very Difference									
Study or Subaroup	Мези	sninenta snin	ai Total	Mean		otal V	Ju Veight	IV Random 95% Cl	IV Random 95% Cl
Awad 2002	27.7	7.0	0	10.2	0.1	0141 1	7.2%	1 05 [ 0 01 2 12]	IV, Kandolii, 95% Ci
Awad 2005 Cüngörmüs 2015	6 29	7.9	0	10.2	9.1	0	1.2%		
Juncosa A 2006	50.2	1 2	12	24.00	2.4	12	4.2%	7.07 [4.74, 9.40]	
Juncosa R 2006	21 1	4.5	12	24.0	2. <del>4</del> 4.1	12	7.6%	0.06 [0.14, 1.78]	
Meimandi A 2013	2 60	0.47	10	0.4	0.11	10	1 7%	6 43 [4 04 8 81]	-
Meimandi R 2013	2.09	0.66	10	2 25	0.11	10	6.8%	2 68 [1 40 3 95]	
Moshiri A 2013	9.08	1 79	10	2.20	2 19	10	6.6%	3 06 [1 69 4 43]	•
Ni 2012	16.42	3.61	19	11 73	2.52	19	7.7%	1 47 [0 75, 2 20]	
Ni 2013	29.21	4.4	10	18.42	4.01	10	6.9%	2.45 [1.23, 3.68]	*
Orvan A 2014	20.48	2.32	10	16.87	1.54	10	7.2%	1.76 [0.69, 2.82]	
Orvan B 2012	18.54	2.32	10	11	1.39	10	6.2%	3.78 [2.20, 5.35]	*
Oryan C 2014	20.57	2.92	10	11	1.39	10	6.1%	4.01 [2.37, 5.65]	*
Oryan D 2014	2.69	0.47	10	0.4	0.11	10	4.7%	6.43 [4.04, 8.81]	+
Shen 2010	7.2	1.7	5	6.7	2.1	5	6.8%	0.24 [-1.01, 1.48]	+
Yokoya 2012	3.04	0.54	8	1.58	0.13	8	6.0%	3.51 [1.80, 5.23]	*
Zhao 2014	1.82	0.03	8	1.65	0.09	8	6.6%	2.40 [1.03, 3.77]	*
Total (95% CI)			158			158 1	.00.0%	2.93 [2.14, 3.72]	
Heterogeneity: Tau <sup>2</sup>	= 1.99; C	$chi^2 = 8$	3.40, 0	f = 15	(P < 0.0	0001);	$1^2 = 82\%$	I	-100 -50 0 50 100
Test for overall effect	t: $Z = 7.2$	24 (P < (	0.0000	1)					Favours [control] Favours [experimental]
							FI	g. 20	
	Expe	erimenta	al	0	Control			Std. Mean Difference	Std. Mean Difference
Study or Subgroup	Mean	SD	Total	Mean	SD SD	Total	Weight	IV, Random, 95% CI	IV, Random, 95% CI
Awad 2003	428.9	151.5	8	238.4	92.2	8	7.9%	1.44 [0.30, 2.57]	*
Güngörmüs 2015	15.6	0.7	5	14.25	1.1	5	7.5%	1.32 [-0.12, 2.77]	ł
Juncosa A 2006	268.7	19.7	12	159.5	12.3	12	6.6%	6.42 [4.28, 8.56]	-
Juncosa B 2006	168.2	34.6	13	139.2	20.2	13	8.2%	0.99 [0.17, 1.81]	
Meimandi A 2013	43.81	4.19	10	4.05	1.28	10	3.9%	12.29 [7.95, 16.63]	
Meimandi B 2013	0.31	0.07	10	0.08	0.03	10	7.2%	4.09 [2.43, 5.75]	ľ
NOSHITI A 2013	120.01	33 57	10	43.81	4.19	10	5.5%	2 12 [1 22 2 05]	. –
Ni 2012	183.05	14 66	10	128.29	11 25	19	7 202	4 04 [2 30 5 60]	ĺ.
Orvan B 2012	1 38	0.23	10	0.53	0 1	10	7.5%	4.59 [2.55, 5.09]	
Orvan C 2014	1.66	0.26	10	0.53	0.1	10	6.7%	5.49 [3.40, 7.59]	-
Orvan D 2014	43.81	4.19	10	4.05	1.28	10	3.9%	12.29 [7.95, 16.63]	-
Pelled 2012	58.2	20.2	10	35.6	0.1	10	8.0%	1.52 [0.49, 2.54]	•
Shen 2010	45.3	10.4	5	32.6	3.9	5	7.5%	1.46 [-0.03, 2.95]	ŀ
Yokoya 2012	5.92	0.73	8	3.5	0.49	5	6.9%	3.45 [1.51, 5.39]	+
I otal (95% Cl) 150 147 100.0% 4.06 [2,90, 5.21]									
Heterogeneity: Tau <sup>2</sup> =	= 4.09; Cł	$11^{\circ} = 113$	8.23, 0	T = 14 (	۲ < 0.00	J001); I	- = 88%		-100 -50 0 50 100
rest for overall effect	L = 0.88	o (r < 0.	00001	,					Favours [control] Favours [experimental]

Fig. 2c

Meta-analysis for a) the maximum load, b) the maximum stress, and c) the Young's modulus of experimental groups and controls.

infraspinatus tendon (two, 5.7%); and digital superficial flexor tendon (two, 5.7%).

In terms of tissue engineering strategies for the treatment of tendon injuries in these studies, we found the following breakdown: stem cells (18, 51.4%); biological scaffolds (seven, 20%); growth factors (five, 14.3%); synthetic biomaterials (four, 11.4%); and a combination of these approaches (one, 2.9%). **Meta-analysis.** Overall, the meta-analysis revealed a statistically significant effect in favour of the maximum load (structural property; standard mean difference of 6.82 N, 95% CI 4.81 to 8.83), the maximum stress (material property; standard mean difference of 2.93 MPa, 95% CI 2.14 to 3.72), and the Young's modulus (mechanical property; standard mean difference of 4.06 MPa, 95% CI 2.90 to 5.21) between experimental and control groups (Fig. 2).



Funnel plot analysis for the publication bias of maximum load (blue), maximum stress (green), and Young's modulus (red) outcomes. Funnel plot analysis indicated a low likelihood of publication bias.

Nevertheless, there was evidence for significant heterogeneity among groups (the l<sup>2</sup> values were >80%, p<0.01). For this reason, we used a random-effects model for analysis.

In these analyses, in the forest plot, the diamonds were on the right side of the vertical line and did not intersect with the line, favouring experimental groups.

**Publication bias assessment.** Funnel plot indicated low likelihood of publication bias (Fig. 3).

#### Discussion

**Animal models.** The selection of animal models is essential to ensure a correct translation to clinical practice. Rats are less expensive and easier to handle and maintain than other laboratory animals. However, their small size reduces the clinical translation of the developed regenerative strategies, but working with them facilitated the histological, functional and biomechanical analyses. Large animals, such as rabbits, dogs, or cows, have high costs and require specialized personnel to handle them, but they are more suitable for testing surgical approaches, techniques, and rehabilitation protocols.<sup>8</sup>

The rat rotator cuff model does not replicate the anatomy and kinematics of the human shoulder, but do share some resemblance. The Achilles and patellar tendons are easy to study using animal models because of their simple surgical approach and the possibility of reproducing tendon injuries and cyclic loads.<sup>9</sup> However, animal models can never replicate human conditions because many of them are quadrupeds and their tendons carry different loads with molecular differences. In addition to anatomical and size differences, histological, potential molecular, and regenerative differences should be considered.

**Tissue-engineered strategies.** Nowadays, an ideal engineered tendon substitute must be biodegradable, biocompatible, and biomechanically stable to support the

tension during healing. Furthermore, the combination of biomaterials and cells must reassemble the native structure of tendon and support the regeneration without adhesions, toxicity, or, tissue rejection.<sup>10</sup>

Tissue engineering approaches to repair and improve tendon healing include: biological and decellularized tissues, the use of natural and synthetic biomaterials, the use of growth factors, stem cell-based therapies, or a combination of these strategies.<sup>11</sup> In addition, there is a growing interest in the use of nanomaterials in tendon tissue engineering, and they could play a key role in tendon healing, as they can act as a carrier for gene therapy or growth factors, and thus help modulate the regenerative function of cells.<sup>12</sup>

An example of a biologic scaffold is the use of porcine small intestinal submucosa. When this biomaterial is implanted, it induces a site-specific tissue repair with a tendon histologically similar to native tendon. However, the use of this scaffold may generate a foreign body and inflammatory reaction.<sup>13</sup> Some authors are focused on the decellularization of tissues and organs in order to reduce the immunogenicity of these grafts, while maintaining the 3D structure and molecular composition of the extracellular matrix.<sup>14,15</sup> In this sense, a reduction of the inflammatory response was observed *in vivo*.<sup>16</sup>

Concerning the use of biomaterials, synthetic ones (such as polyglycolic acid) resulted in biomechanically and structurally stable tendon graft that supports tendon cell migration, especially those subjected to crosslinking.<sup>17</sup> Similarly, chitosan-based hyaluronan hybrid fibre scaffolds have been used in tendon repair with better collagen type I production.<sup>18</sup> Polyhydroxyalkanoates are a family of biopolymers with adaptable mechanical properties and delayed biodegradability.<sup>19</sup>

Collagen type I, the main component of the tendon, has been shown to have an excellent biocompatibility and biodegradability; with nanostructured and crosslinking technologies, it is possible to polymerize the type I collagen to produce effective scaffolds.<sup>20</sup> Electrospinning of collagen fibres produces elaborate nanofibres with the desirable size, density, and alignment.<sup>21</sup>

Bone marrow and adipose mesenchymal stem cells (MSCs) are a commonly used cell source in musculoskeletal and peripheral nerve tissue engineering due to their ability to differentiate and their easy isolation and culture.<sup>4,22,23</sup> When these cells were used in tendon repair, they improved tendinous healing in short-term studies. However, these studies suggest that no significant differences can be observed in long-term comparative studies; this could be related to the high regeneration capability of the animal models used.<sup>24-26</sup> Tendon-derived stem cells have higher mRNA expression of tenomodulin, scleraxis, type I collagen and decorin than that of MSCs, and could promote earlier and better tendon healing. On the other hand, in published studies, the biomechanical properties of the native tendon have never been restored successfully using tendon-derived stem cells.<sup>27</sup> In addition to the regenerative potential of adipose-derived stromal cells, it was recently reported that these cells promote neoangiogenesis, cell proliferation and extracellular matrix (ECM) remodelling, and that they protect the regenerative microenvironment from macrophages.<sup>28</sup>

Growth factors, which are produced by antiinflammatory macrophages, play a key role in the regulation of all phases of tendon healing because they are needed to activate different cellular processes (such as proliferation, differentiation, and migration) and to increase the synthesis of crucial ECM.<sup>29</sup> These factors can be delivered to the regenerative microenvironment by direct application or by using impregnated sutures for slow release, or a scaffold-based delivery system.<sup>30</sup> Basic fibroblast growth factor (bFGF) has a beneficial effect on tendon healing by regulating cellular migration, promoting angiogenesis, and inhibiting inflammatory processes.<sup>31</sup> Bone morphogenetic protein 2 (BMP2) was involved in tendon differentiation and maintenance, modulating collagen formation, and tendon remodelling.<sup>32,33</sup> Another example is the connective tissue growth factor (CTGF) that is highly expressed in the early stage of tendon repair and can promote tendon repair.<sup>34</sup> Plateletrich plasma (PRP) was recently introduced as a novel treatment for tendon injuries that would enhance the synthesis of type I and type III collagen and would limit matrix degradation.<sup>35,36</sup> Stromal cell-derived factor-1 alpha (SDF-1 $\alpha$ ) is a cytokine that regulates inflammatory cell recruitment and could improve the structural and biomechanical characteristics of repaired tendon.<sup>37</sup>

Gene therapy is another attractive field in tissue engineering but it is still necessary to define optimal cell targets and identify genes whose modification has a significant therapeutic response.<sup>38</sup>

There are several strengths in this meta-analysis. This is the first study that showed favourable outcomes when using tissue engineering strategies in the treatment of tendon injuries in animal models. Therefore, the quality assessment score for most of the included studies was high, favouring the results of the meta-analysis. Nevertheless, there are a series of limitations associated with this work. First, like any systematic review, the conclusions of our work are affected by the quality of studies included. However, most included studies in this work had a high quality according to ARRIVE guidelines. Second, our search strategy may associate search bias due to this is an English language-only revision, which entails language bias. On the other hand, the results on animal model have a limited value for a human application.

In conclusion, at present, there are numerous gaps in the basic science of tendon healing. As a result, the orthopaedic surgeon has few solutions at his fingertips in the event of a tendon injury. In recent years, thanks to tissue engineering techniques and the use of animal models, we have growth factors, scaffolds, and stem cells that can improve the histological and biomechanical characteristics of repair tissue, but do not fully recapitulate the native tendon.

## **Supplementary material**

A table showing benefits and limitations of tissue engineering strategies for tendon injuries

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#### Author Contributions

- D. González-Quevedo: Online research and abstract selection, Analyzing and interpreting the data, Writing the manuscript.
- I. Martínez-Medina: Online research and abstract selection.
- A. Campos: Supervising the study.
  F. Campos: Critical revision of the manuscript.
- F. Campos: Critical revision of the manuscript
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#### **Conflict of Interest Statement**

None declared.

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